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UNIT 5: Adaptive filtering

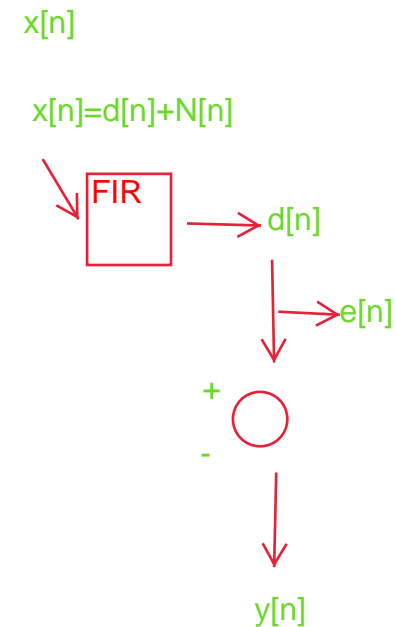
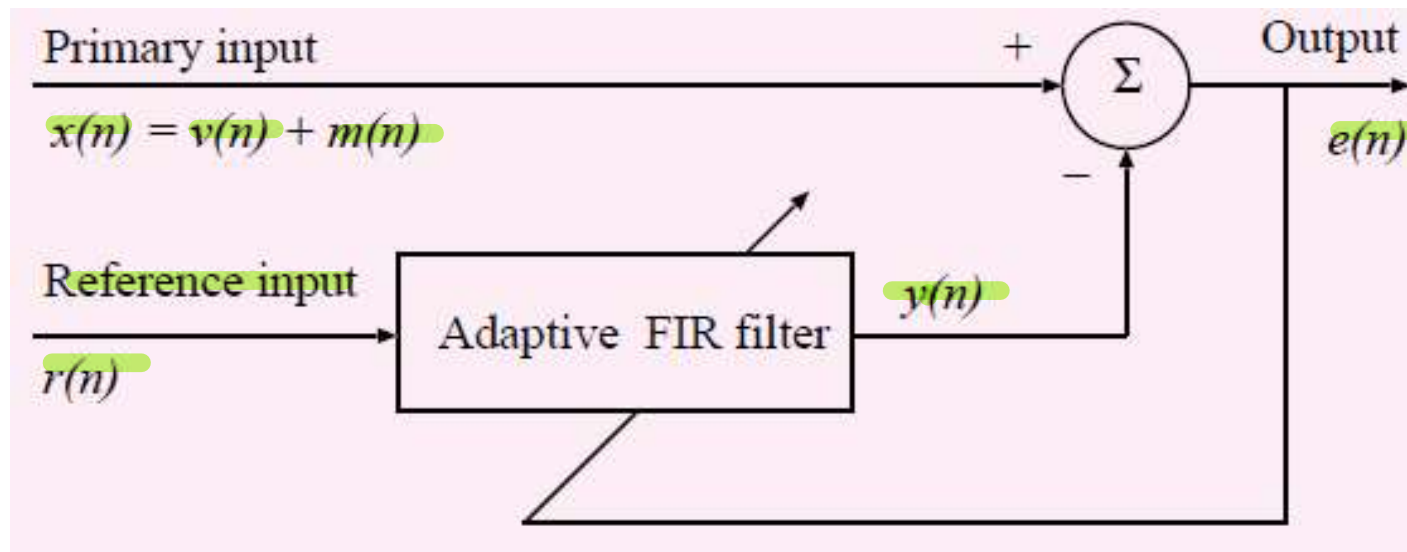
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(based on “Biomedical Signal Analysis”, 2nd edition, © Willey 2015)

Adaptive filtering

- Wiener filters provides a means to design optimal filters given that the statistics of the desired signals and the noise are known
- The Wiener filtering theory can be extended to the design of adaptive filtering, that is filters that modify their coefficient in order to optimize a quality criterium
- Adaptive filters enable working with unknown and not necessarily stationary signals
- In this unit we focus on the **adaptive noise canceller (ANC)**

Adaptive noise cancelling



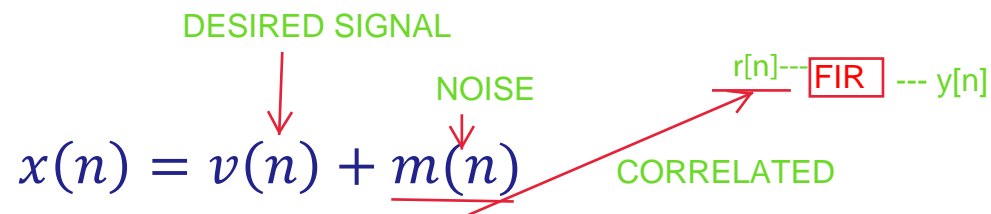
- The *primary input* is composed of the desired signal $v(n)$ a noise $m(n)$, both uncorrelated and with zero mean
- The *reference $r(n)$ input* has zero mean and it is correlated with $m(n)$ and uncorrelated with $v(n)$
- The filter produces $y(n)$ which is an estimation of noise $m(n)$
- Subtracting the estimation of the noise to $x(n)$ leads to $e(n)$, an estimation of the desired signal $v(n)$

Adaptive noise cancelling

- We are going to follow an approach very similar to that of Wiener filtering

Minimized the MSE, considering that $\mathbf{e}(n)$, which is the estimate of $\mathbf{v}(n)$, is the error

- The primary input is



- The output signal is

$$e(n) = x(n) - y(n) = \underbrace{v(n)}_a + \underbrace{m(n) - y(n)}_b = v(n)$$

- The MSE is

$$MSE = E[e^2(n)]$$

$$= E[v^2(n)] + E[\{m(n) - y(n)\}^2] + \overbrace{2E[v(n)\{m(n) - y(n)\}]}^{\text{uncorrelated}} = 0$$

$$= E[v^2(n)] + E[\{m(n) - y(n)\}^2]$$

$v(n)$ has zero mean and it is uncorrelated with $m(n)$ and $y(n)$

Adaptive noise cancelling

$$\text{MSE} = \overset{\text{-----FIXED-----}}{E[v^2(n)]} + \overset{\text{-----RELATED TO THE FILTER'S COEFFICIENT}}{E[\{m(n) - y(n)\}^2]}$$

- So, to minimize MSE we have to minimize

$$y[n] = m[n]$$

$$E[\{m(n) - y(n)\}^2]$$

- Thus, once the system is minimized the estimation $\mathbf{y(n)}$ is the minimum MSE estimate of $m(t)$
- As consequence, $\mathbf{e(n)}$ is also the minimum MSE estimate of $\mathbf{v(n)}$
- Minimizing the estimation error of the noise, maximizes the SNR at the output

Adaptive noise cancelling

- Let us now introduce vectors to obtain more compact expressions

$$\vec{w} = [w_0, w_1, w_2, \dots, w_{M-1}]^T \quad M \text{ coefficients}$$

$$\vec{r}(n) = [r(n), r(n-1), \dots, r(n-M+1)]^T$$

current value

- The output of the system is |-----(m-1) past values-----|

$$e(n) = x(n) - \vec{w}^T \vec{r}(n)$$

$y[n]$

- There are several methods to minimize $\mathbf{e}(\mathbf{n})$ in real-time
- Note that the only constraint that we are imposing is that of the correlation level between $\mathbf{m}(\mathbf{n})$, $\mathbf{r}(\mathbf{n})$ and $\mathbf{v}(\mathbf{n})$, and that the means are all zero
- We will focus on the **Least Mean Squares** method (**LMS**)

The LMS adaptive filter

- The aim of the LMS filter is to minimize the squared error, assuming that the current squared error is a good approximation of the MSE $a^T * b = b^T * a^*$

$$MSE = E[e^2(n)] \approx e^2(n)$$

- Therefore, the filter is continuously minimizing $e^2(n)$

$$\begin{aligned} e^2(n) &= (x(n) - \vec{w}^T \vec{r}(n))(x(n) - \vec{r}^T(n) \vec{w}(n)) \\ &= x^2(n) - 2x(n) \vec{r}^T \vec{w}(n) + \vec{w}^T(n) \vec{r}(n) \vec{r}^T(n) \vec{w}(n) \end{aligned}$$

- The squared error is a hyper-paraboloidal (bowl-like) that is never negative
- The aim of the LMS algorithm is to reach the bottom of the “bowl”
- Since we are not optimizing the MSE but the squared error, there is no need to solve the Winer-Hopf equations
- We resort to the **steepest descent algorithm** to find the minimum

The LMS adaptive filter

$$e^2(n) = x^2(n) - 2x(n)\vec{r}^T\vec{w}(n) + \vec{w}^T(n)\vec{r}(n)\vec{r}^T(n)\vec{w}(n)$$

- Given the current filter coefficients $\mathbf{w}(n)$, the next set of coefficients $\mathbf{w}(n+1)$ is corrected considering the negative of the gradient of $e^2(n)$

$$\vec{w}(n+1) = \vec{w}(n) - \mu\nabla e^2(n)$$

- The parameter μ controls the stability and the rate of convergence

small $\mu \rightarrow$ high stability \rightarrow slow convergence

high $\mu \rightarrow$ low stability \rightarrow fast convergence

- Moreover, the gradient is estimated through the first order derivative

$$\nabla e^2(n) \approx -2x(n)\vec{r}(n) + 2\{\vec{w}^T(n)\vec{r}(n)\}\vec{r}(n) = -2e(n)\vec{r}(n)$$

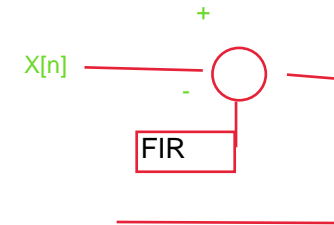
- Thus, the weights are updated as follows

$$\vec{w}(n+1) = \vec{w}(n) + 2\mu e(n)\vec{r}(n)$$

Example: ECG and EMG

- We consider an ECG $v(n)$ signal that is corrupted due to muscular activity ($m_1(n)$) and noise ($n_1(n)$)

$$\begin{aligned}x(n) &= \overset{\text{ECG}}{v(n)} + \overset{\text{EMG}'}{m(n)} \\m(n) &= \underset{\text{EMG}}{m_1(n)} + \underset{\text{noise}}{n_1(n)}\end{aligned}$$



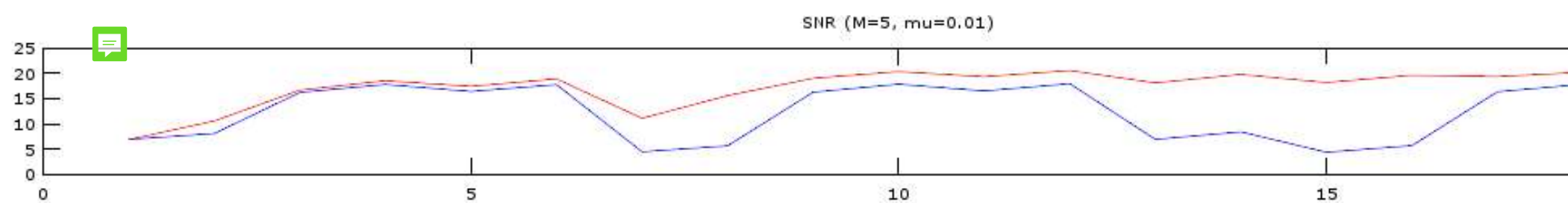
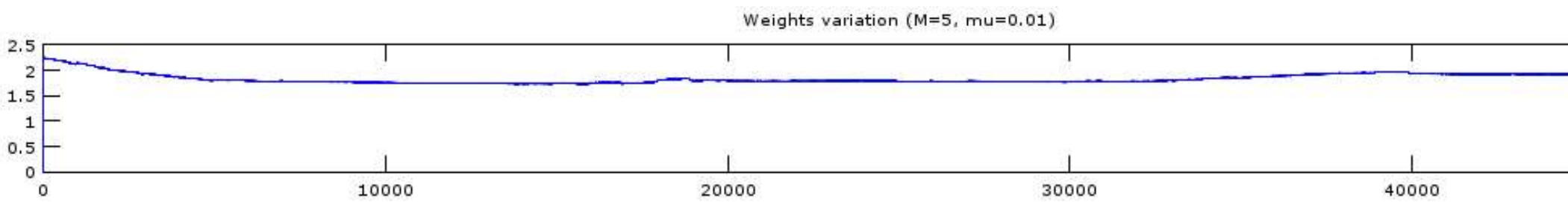
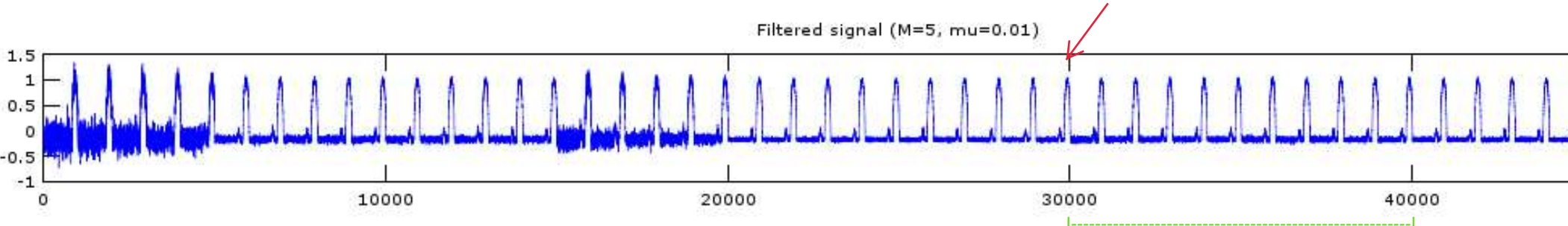
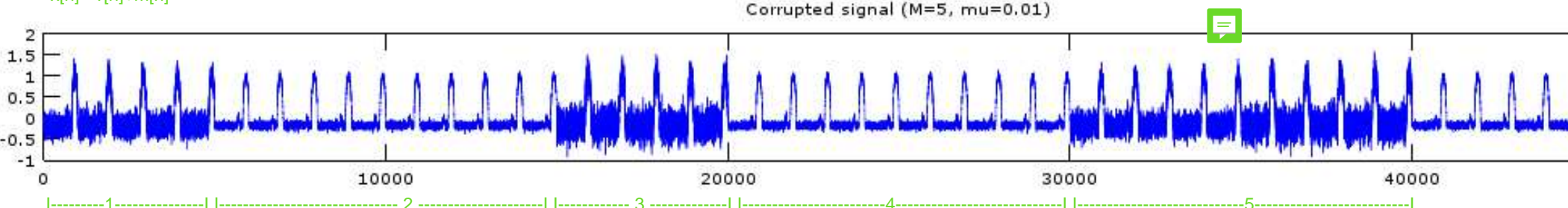
- The secondary input $r(n)$ is the muscular activity obtained through an EMG sensor. This signal is corrupted with noise

$$\underset{\text{EMG}'}{r(n)} = k \cdot \underset{\text{EMG}}{m_1(n)} + \underset{\text{noise}}{n_2(n)}, 0 < k < 1$$

Example: ECG and EMG

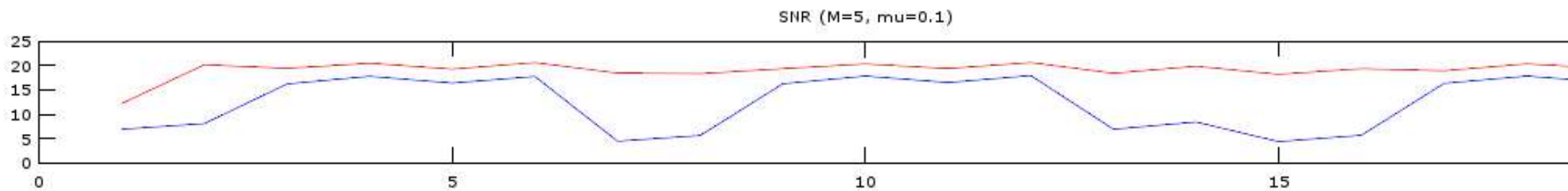
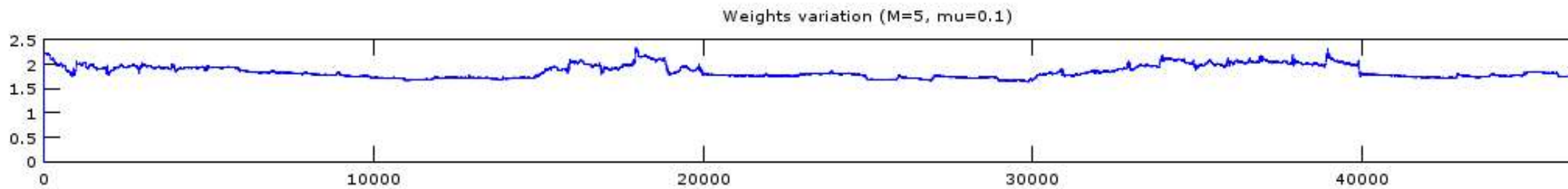
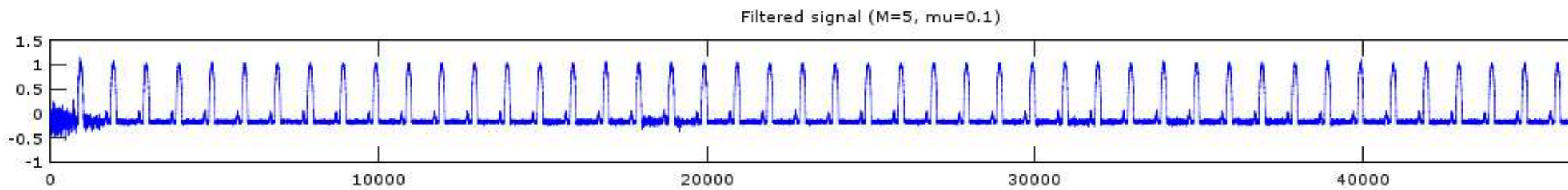
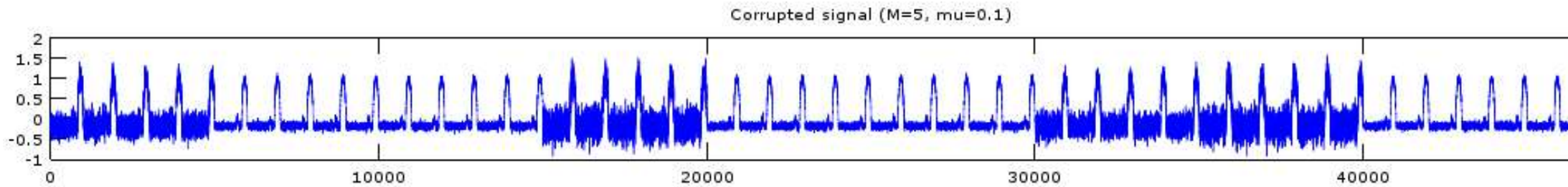
M=5, mu=0.01

$$x[n] = v[n] + m[n]$$



Example: ECG and EMG

$M=5, \mu=0.1$

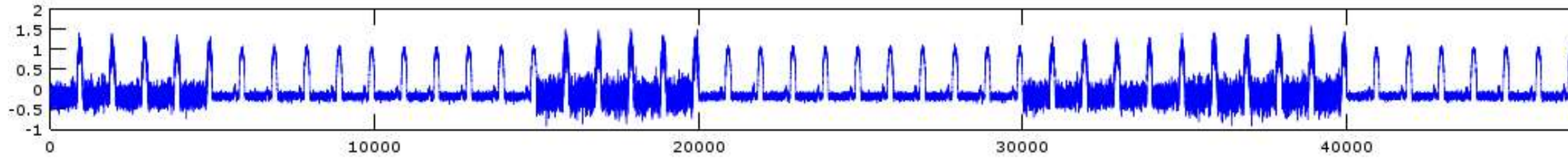


Example: ECG and EMG

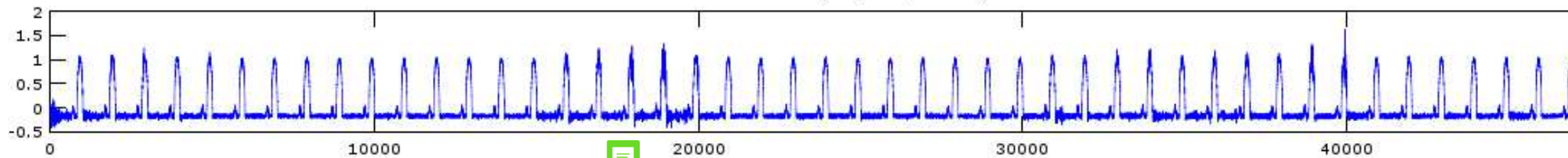
$M=5, \mu=0.5$



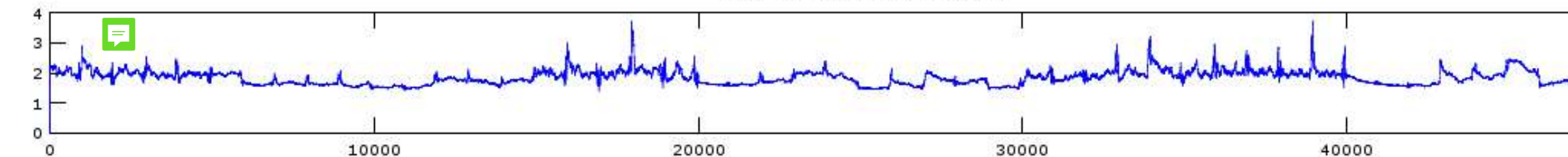
Corrupted signal ($M=5, \mu=0.5$)



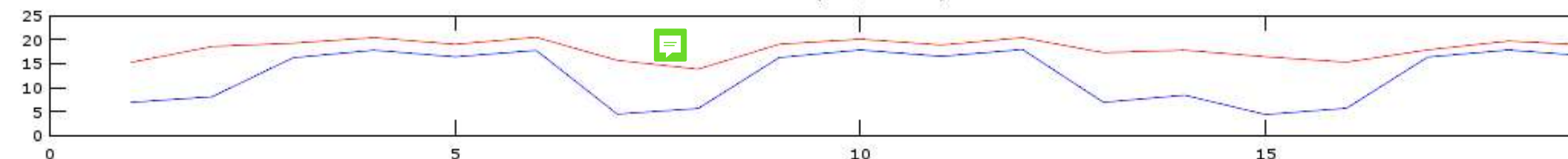
Filtered signal ($M=5, \mu=0.5$)



Weights variation ($M=5, \mu=0.5$)



SNR ($M=5, \mu=0.5$)



SUMMARY

- Adaptive filtering
- LMS filter
- ECG example